### Parameter selection affects the local divergence exponent classification of multiple sclerosis

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## **Summary**

The local divergence exponent (LDE) is a sensitive gait metric in early-stage multiple sclerosis (MS). We compared the MS classification ability of the LDE calculated using different parameter selections (embedded dimensions and time delay) for state-space reconstruction: individual per trial, sample median, and fixed. The best classification of people with (pwMS) was achieved when using the sternum mediolateral direction and a fixed m=5 and  $\tau=10$ .

## Introduction

There is still a need for more sensitive mobility biomarkers of MS progression [1]. The short-term local divergence exponent (LDE; or Lyapunov), which assesses walking stability, has been proposed as a more sensitive measure of MS progression at early stages compared to standard metrics (e.g. speed) [2]. However, calculating the LDE relies on the selection of two main parameters for state-space reconstruction: dimensions (m) and time delay (t) [3]. Here we investigated how parameter selection affects the classification of pwMS at early stages of the disease.

# Methods

33 pwMS with no evident gait dysfunction at clinical examination (EDSS<3.5) and 23 healthy controls (HC) performed a 6-minute walking test while wearing a set of 4 IMUs on the sternum, lumbar area, and feet. Tests were conducted in a 20-meter corridor of an outpatient clinic. Turns were removed from data and walking episodes were used to extract 150 consecutive strides. To reconstruct the state-space, 3 commonly used sets of embedded dimensions (m) and time delay (t) were utilized to calculate the LDE: 1) m and  $\tau$ individually calculated for each trial (individual), 2) m and  $\tau$ median across all pwMS and HC trials (median), and 3) fixed m=5 and  $\tau=10$  (fixed). The LDE was calculated separately for each direction's acceleration (VT, ML, and AP) and the norm (N) acceleration, as well as in 3D, using 2 fixed m=3 and m=5with a  $\tau = 10$ , for both sternum and lumbar sensors using the Rosenstein's algorithm [2]. For each parameter selection method, we applied QDA to classify pwMS versus HC. The dataset was randomly split into training and testing sets with a 2:1 ratio. We then calculated the classification accuracy on the test set and averaged the results over 1,000 random splits.

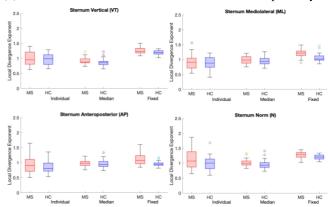
## **Results and Discussion**

Overall, the results show a better classification accuracy when using LDEs calculated using sternum sensor timeseries

compared to lumbar. This is similar to our previous findings [1,2]. The best classification of pwMS was achieved when using the sternum ML LDE obtained with a fixed m=5 and  $\tau$ =10 (78% accuracy). The second best was the sternum 3D LDE a fixed m=5 and  $\tau$ =10 (67% accuracy). Table 1 and figure 1 present accuracy and descriptive statistics, respectively.

	AP	ML	VT	N	3D*
			Lumbar		
I	0.532	0.530	0.513	0.555	0.630
M	0.573	0.549	0.544	0.583	0.600
$\boldsymbol{F}$	0.544	0.538	0.551	0.589	
			Sternum		
I	0.511	0.498	0.505	0.505	0.627
Μ	0.570	0.543	0.552	0.587	0.668
F	0.528	0.777	0.684	0.628	

**Table 1**: Accuracy results using individual (I), median (M) and fixed (F) m and  $\tau$ . \* I and M are fixed with m=3 and m=5, respectively.



**Figure 1**: Sternum LDE for each direction using the 3 m and  $\tau$  sets.

#### Conclusions

The best classification of pwMS was achieved when using the sternum mediolateral direction and with a fixed m=5 and  $\tau=10$ . Using fixed m and t values can facilitate the clinical implementation of the LDE by reducing calculation steps and standardizing procedures for comparison across studies.

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#### References

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